

***Nanoscale Design of Biosensors for
Toxicity Screening and Biomedical
Applications***

James F. Rusling

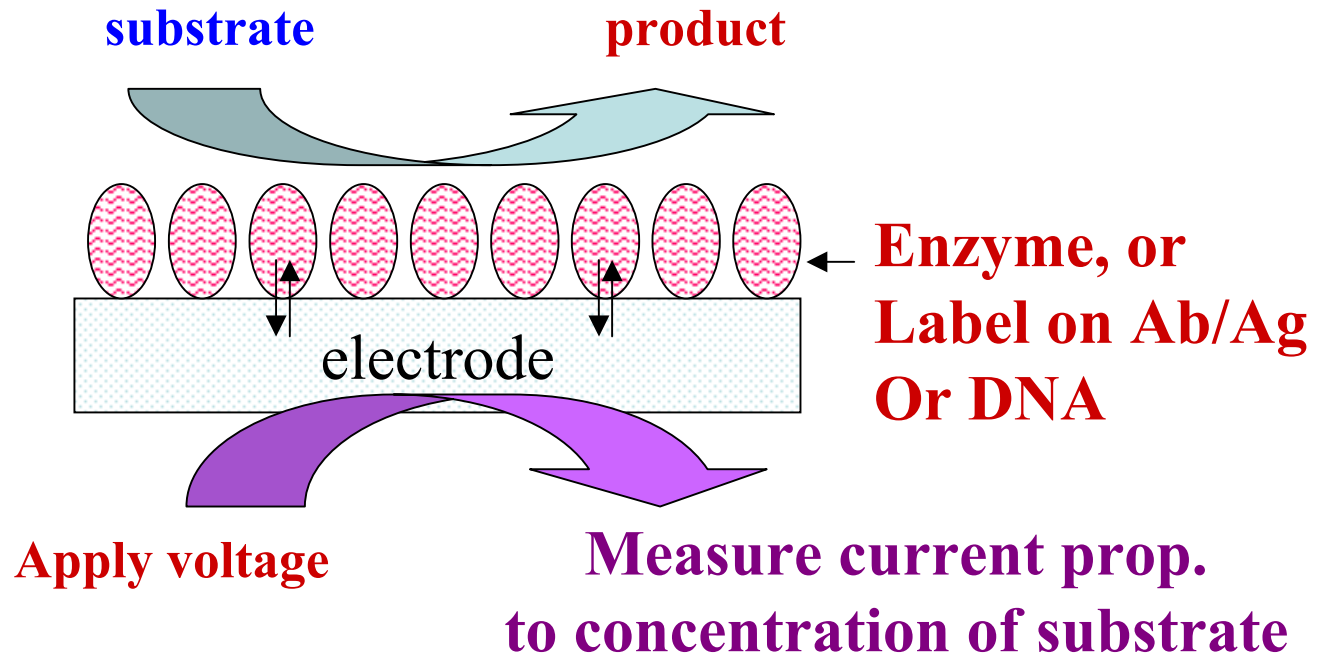
Departments of Chemistry & Pharmacology

University of Connecticut

Storrs, CT, USA



Traditional Electrochemical Biosensors



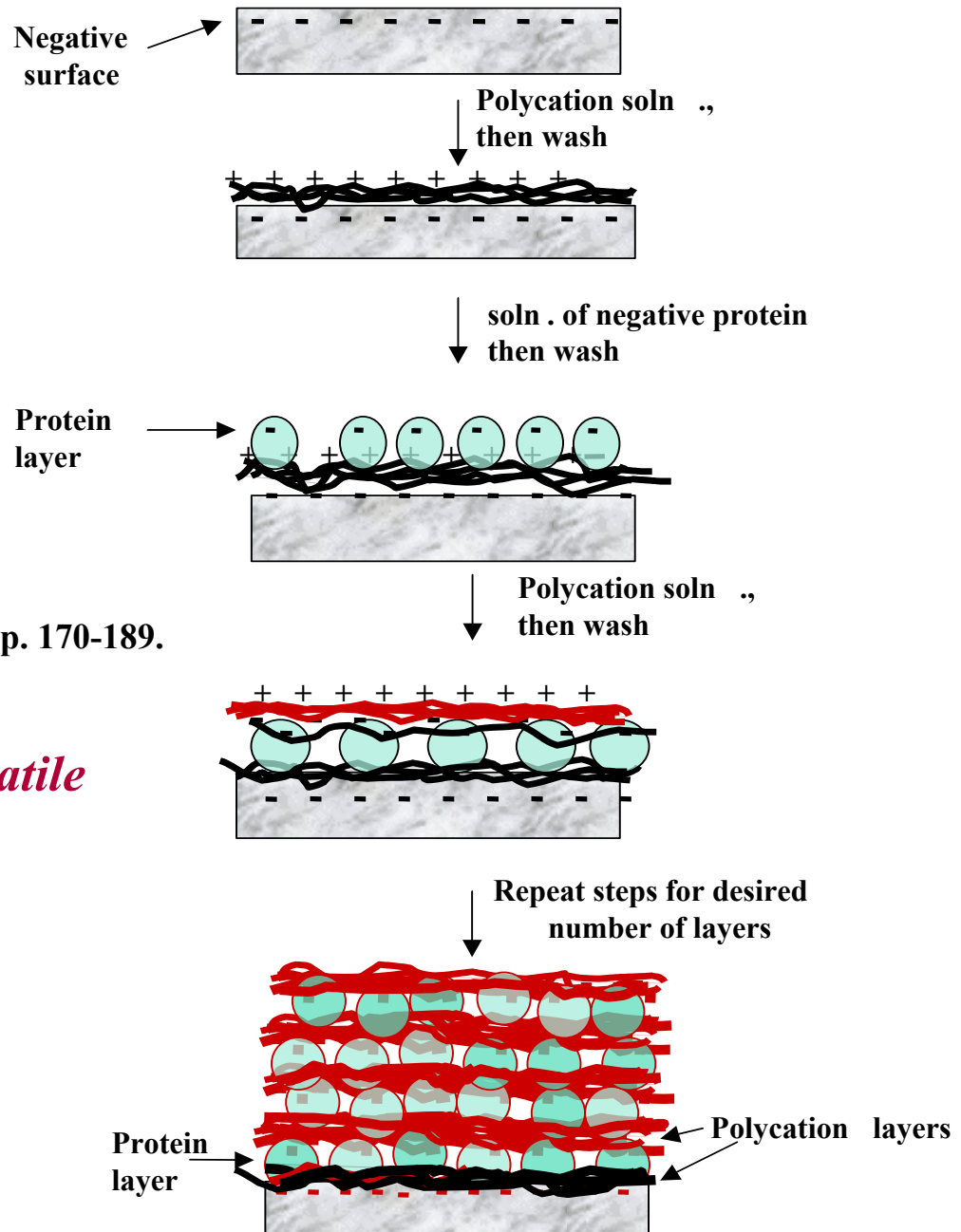
- nanoscale biosensing architecture
- patternable nanomaterials for arrays

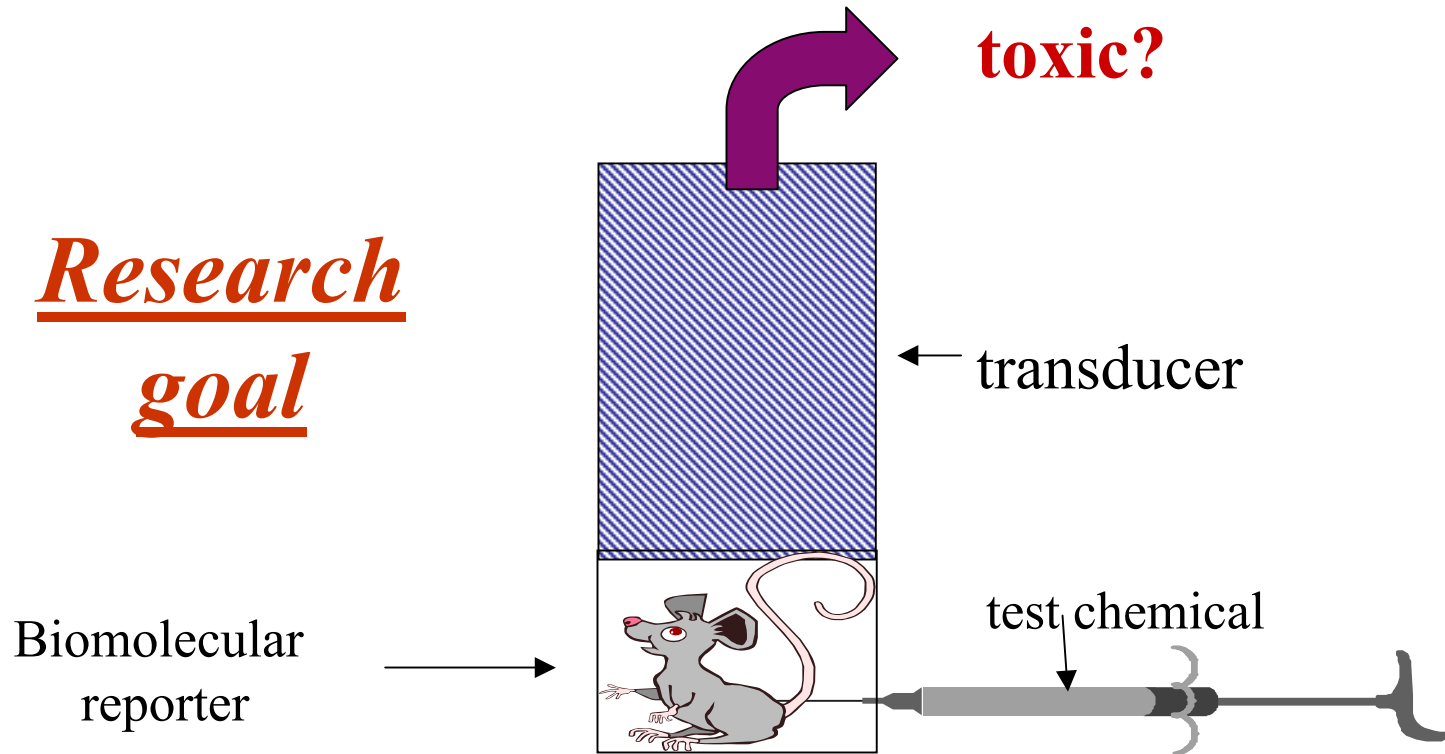
Layer-by-layer Film assembly

Lvov, Decher

Lvov, Y. in Nalwa, R.W.; Ed.;
*Handbook Of Surfaces And Interfaces
Of Materials, Vol. 3.* Academic, 2001, pp. 170-189.

Stable, easily prepared, versatile





- *~ 30 % of drug candidates defeated by toxicity*
- *Early screening could save drug development costs*

In vitro Toxicity Screening

Lipophilic Molecule



← **Cyt P450, O₂** →

Enzyme-activated molecule

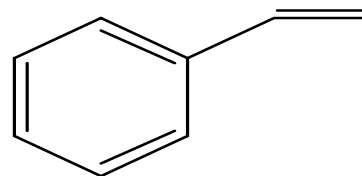


+DNA

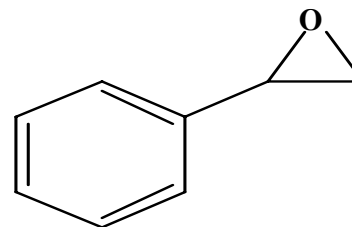
**Damaged
DNA**



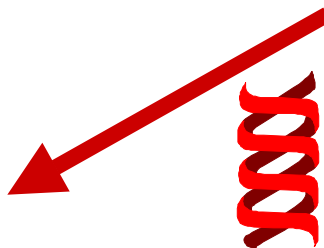
**Detect by electrochemical sensor
Validate by LC-MS/MS**

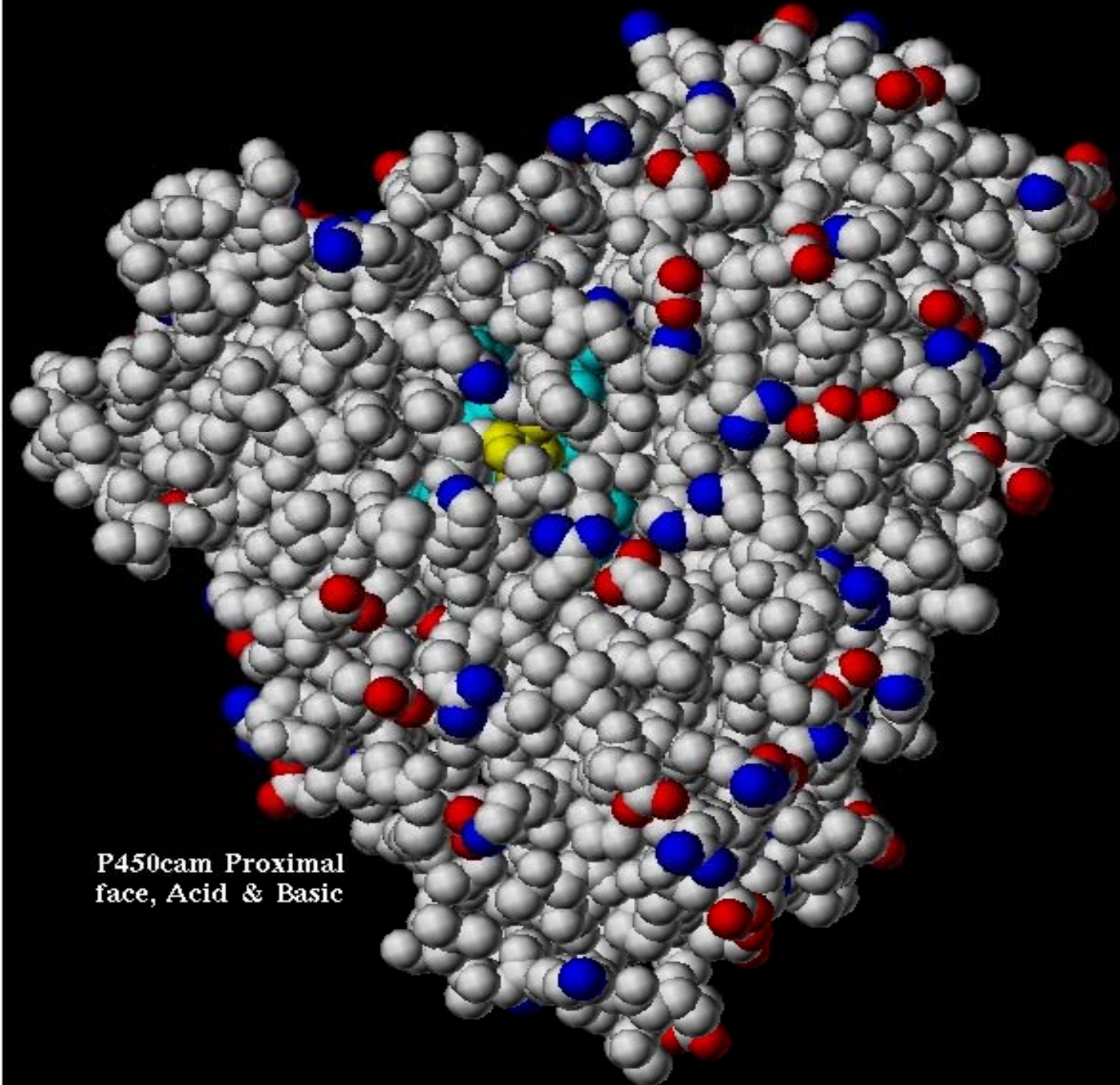


styrene



styrene oxide



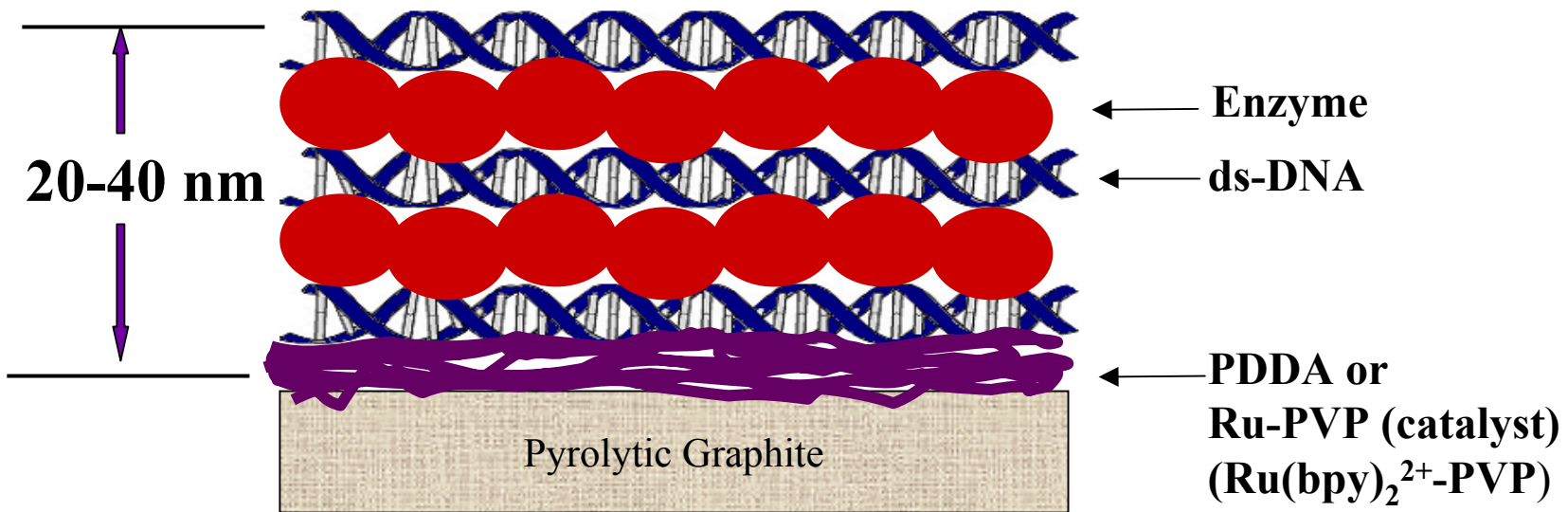


P450cam Proximal
face, Acid & Basic

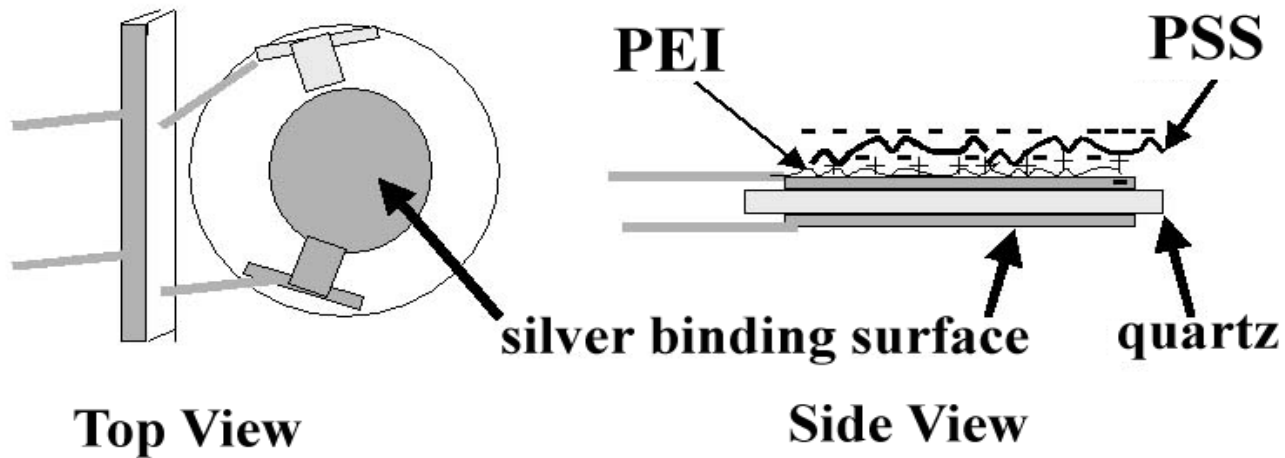


*Collaboration with Prof. John Schenkman,
Pharmacology, Uconn Health Center
Funding from NIH, NIEHS*

Films for Toxicity Screening



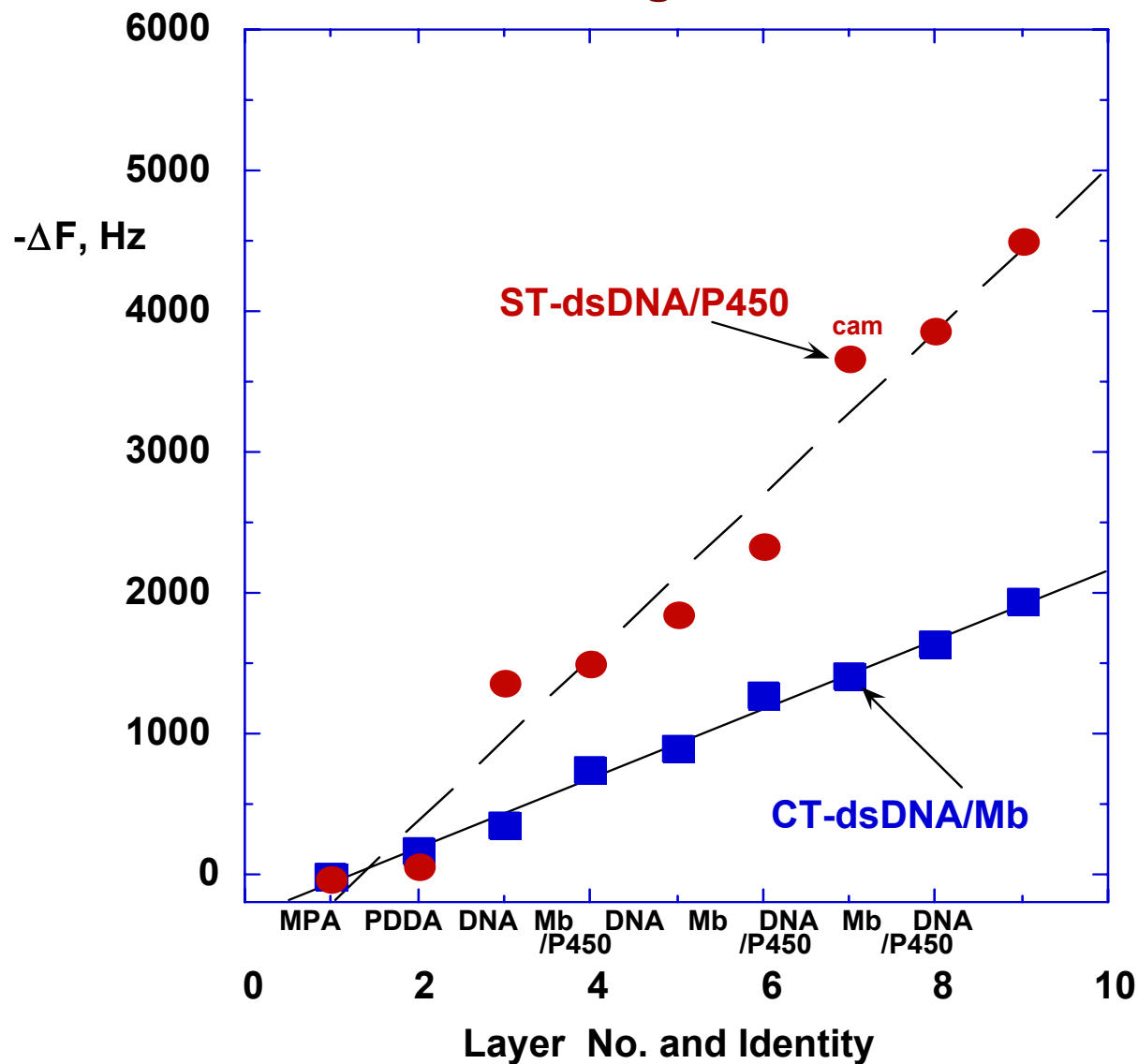
QCM Resonator



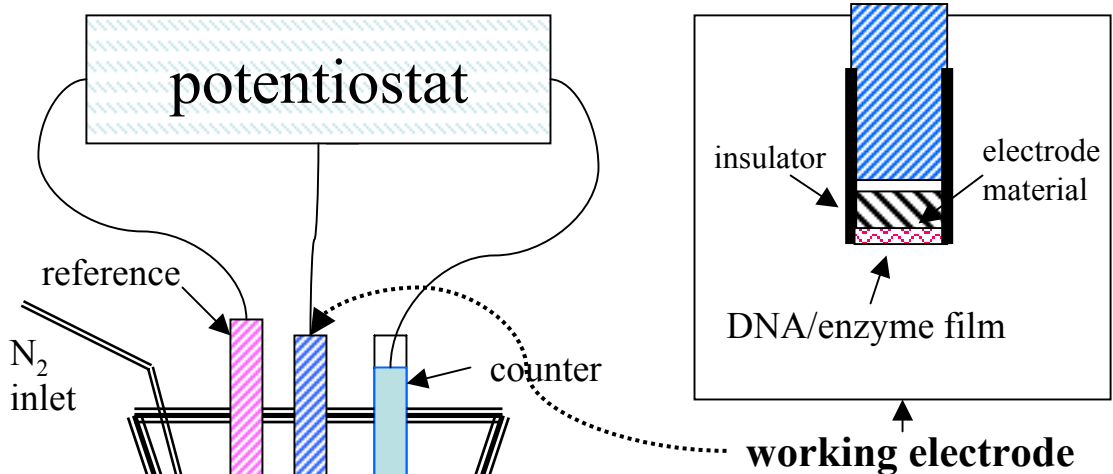
Mass: $M/A = -\Delta F / 1.86 \times 10^8$

Thickness: $d = -(0.016) \Delta F$

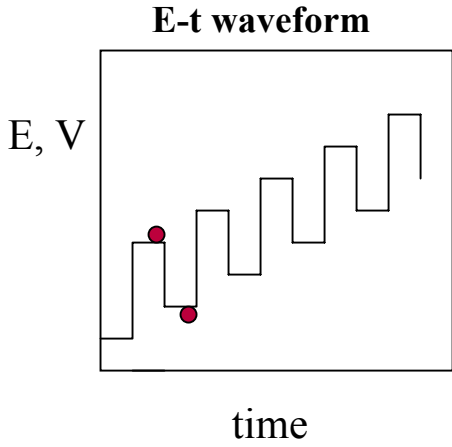
QCM -film growth



Equipment for toxicity biosensors



Electrochemical cell



Square-wave voltammetry

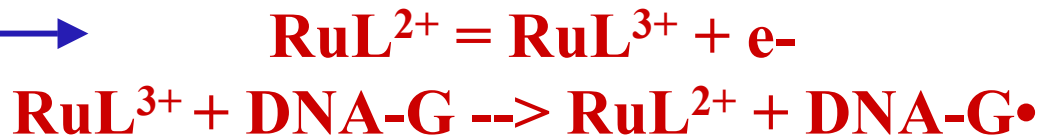
● I measured, then subtracted

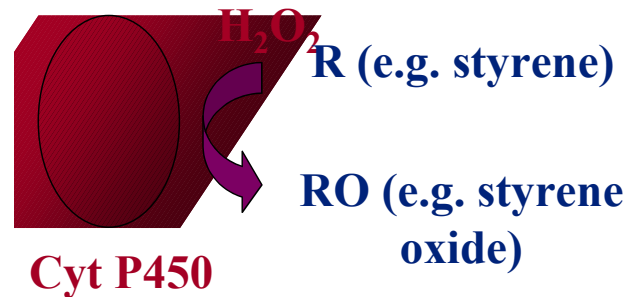
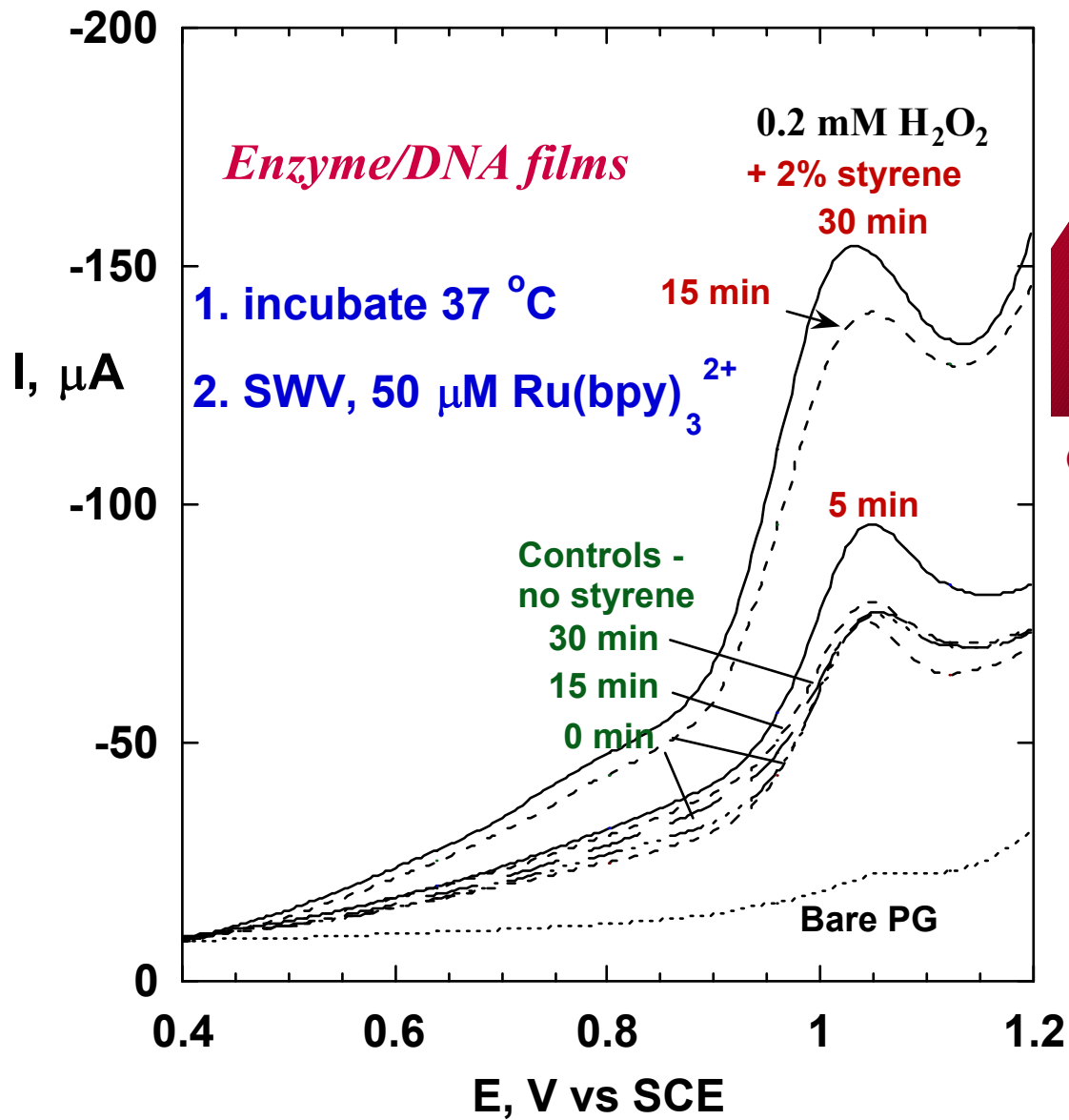
Screening Chemical Toxicity

Enzyme reaction - Incubate:
Reactant + H₂O₂ --> metabolite



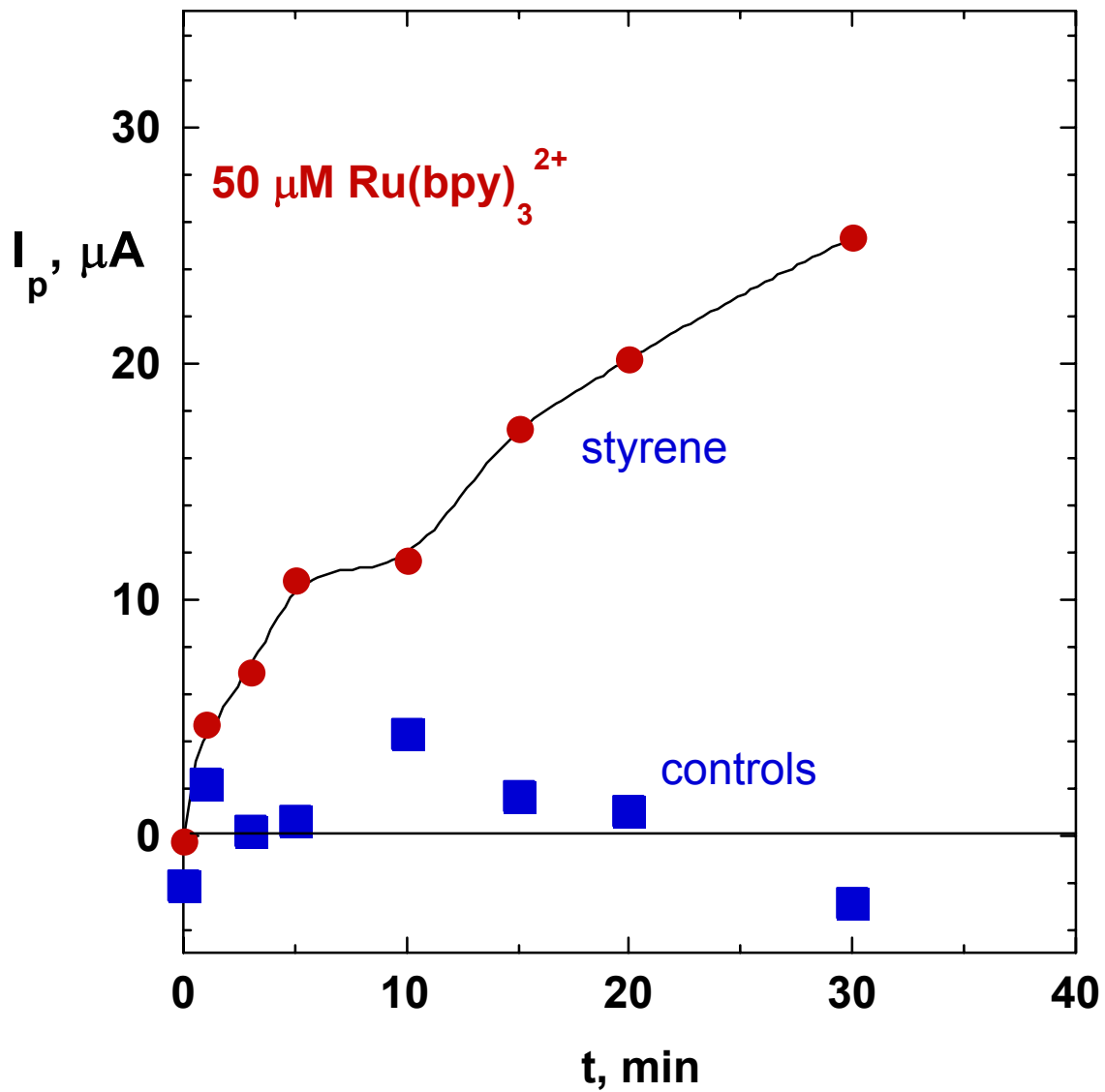
Analysis by catalytic SWV or
electrochemiluminescence



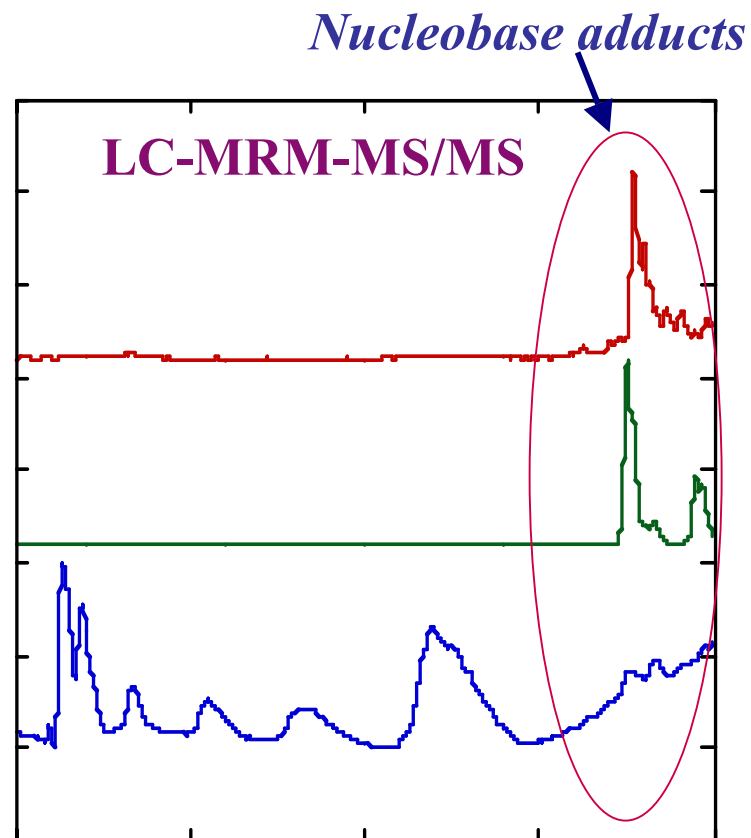
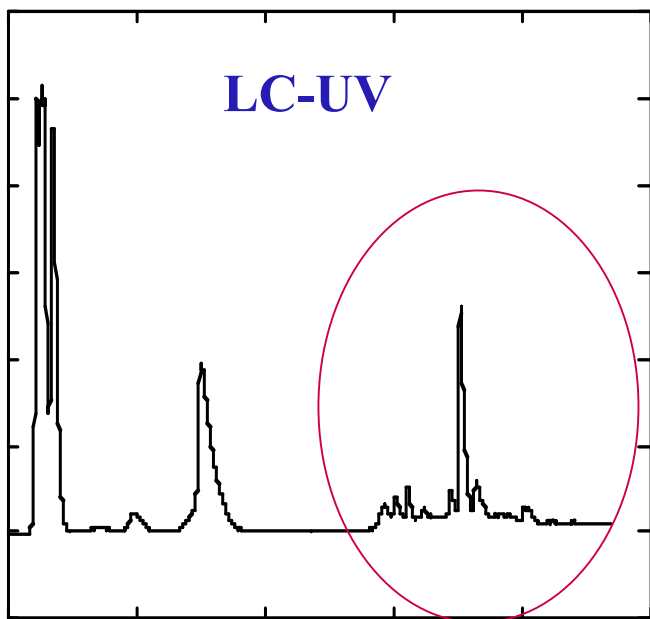


*Peak increase
measures damage
of DNA by enzyme-
generated
metabolite*

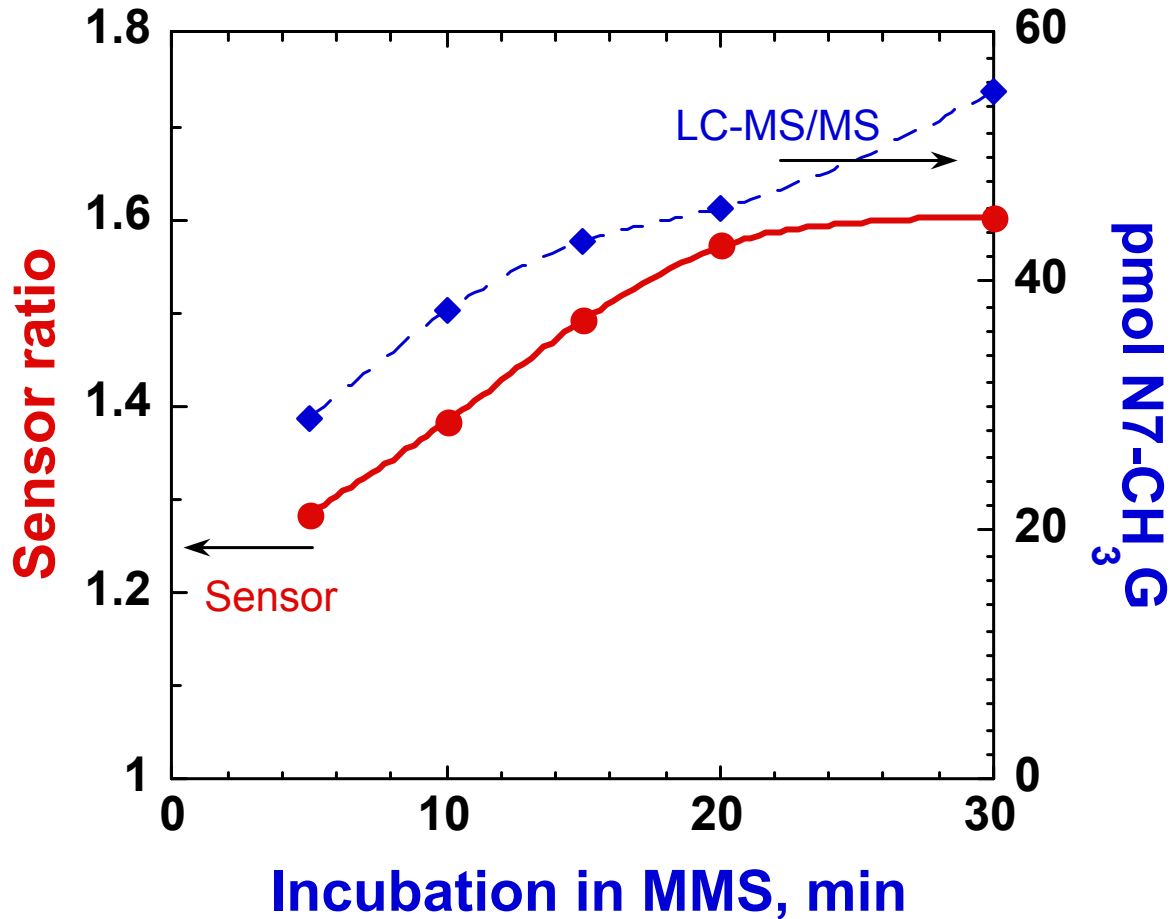
Cyt P450cam/DNA film + 0.2 M H_2O_2



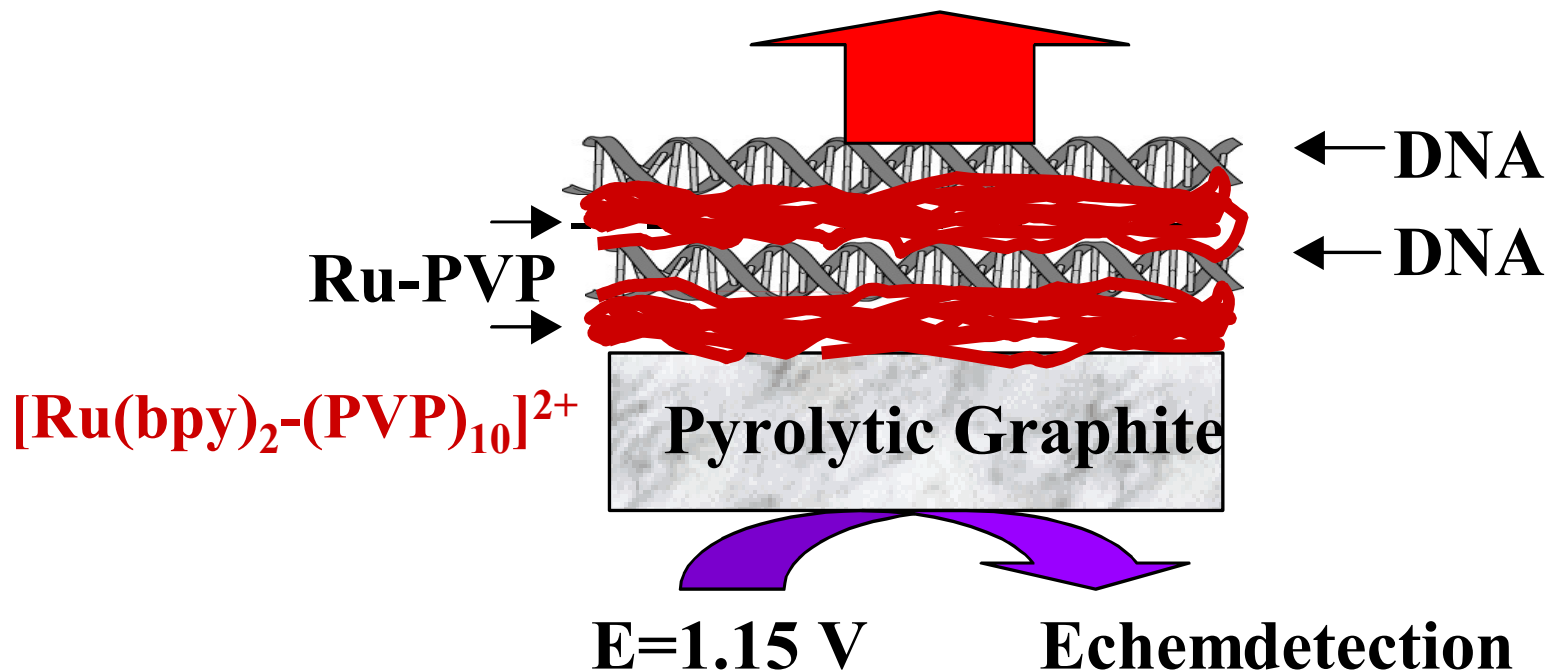
Detection of DNA-styrene oxide adducts after incubations of films + hydrolysis



*Comparison of toxicity sensors with LC-MS
For DNA damage by methylmethane sulfonate*



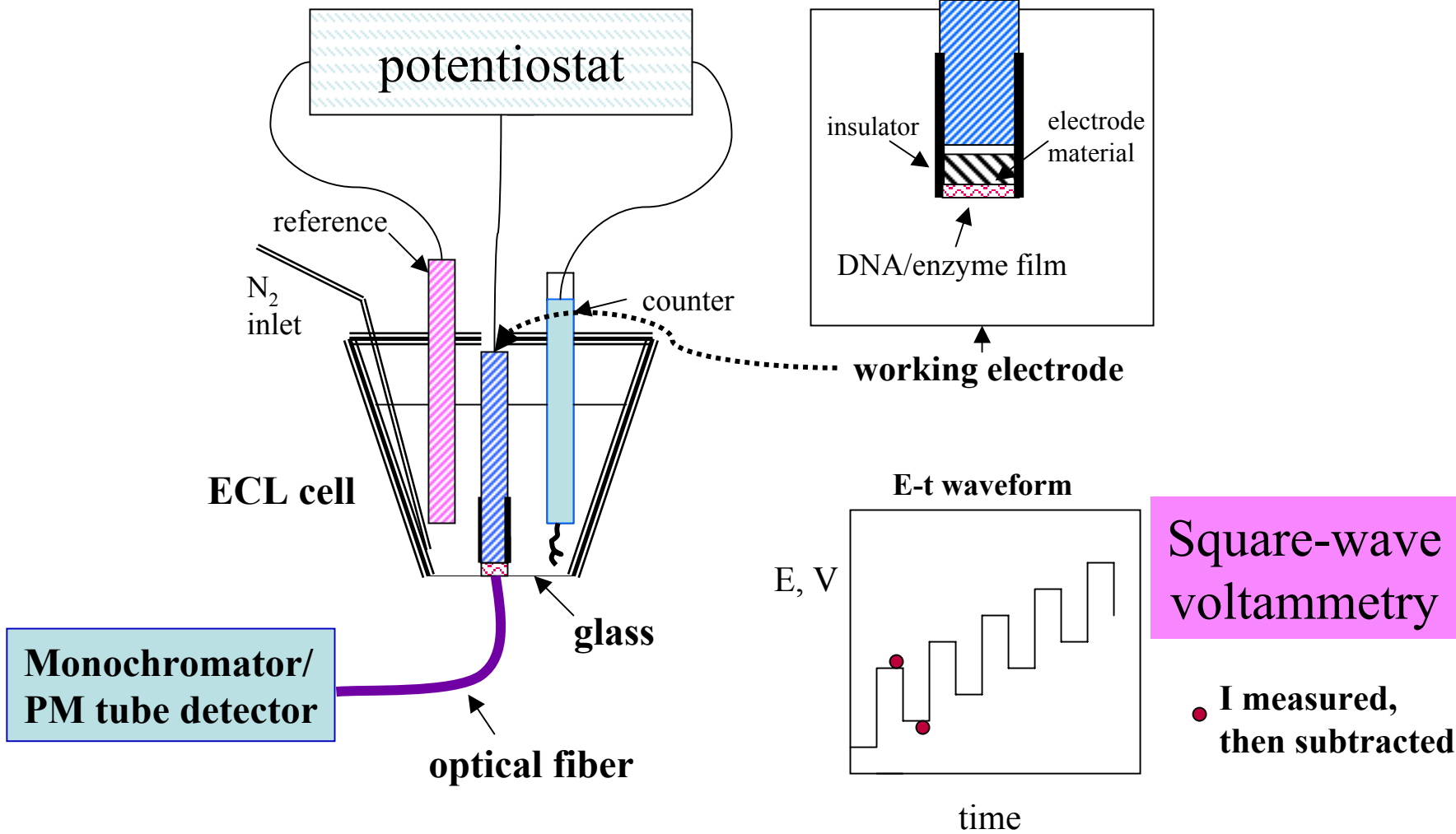
electrochemiluminescence



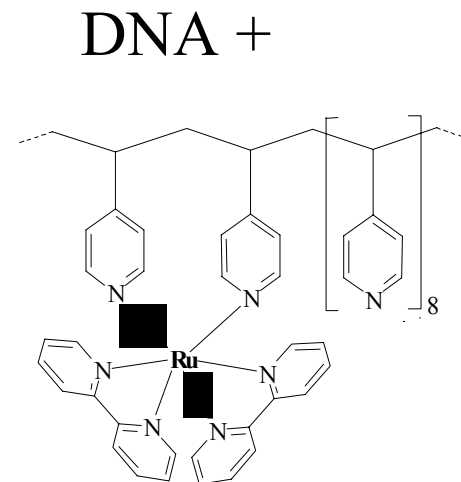
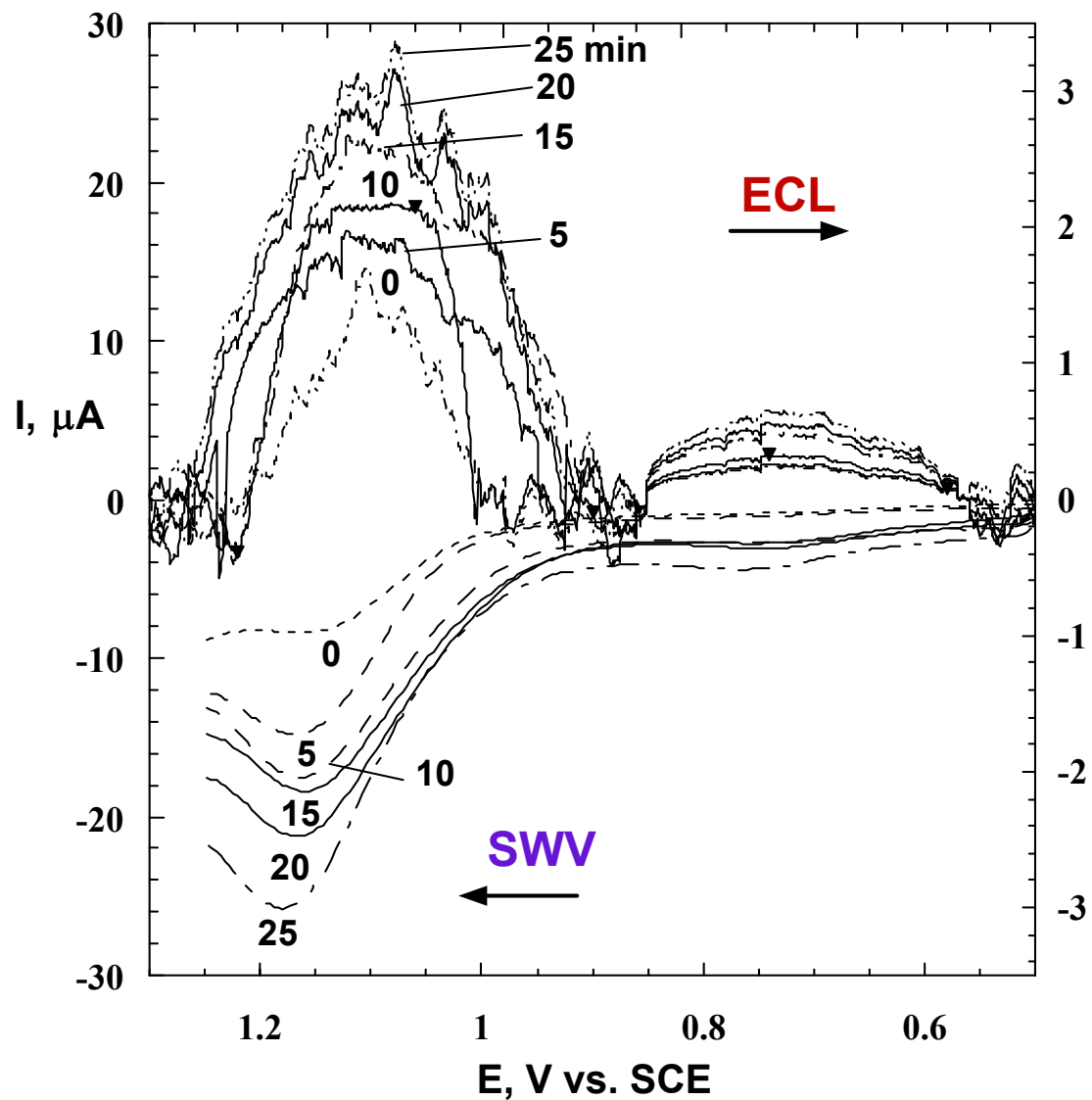
Lynn Dennany, Robert J. Forster and James F. Rusling,
"Simultaneous Direct Electrochemiluminescence and Catalytic
Voltammetry Detection of DNA in Ultrathin Films"
J. Am. Chem. Soc. **2003**, *125*, 5213-5218.

Collaboration with NCSR, Dublin City Univ.

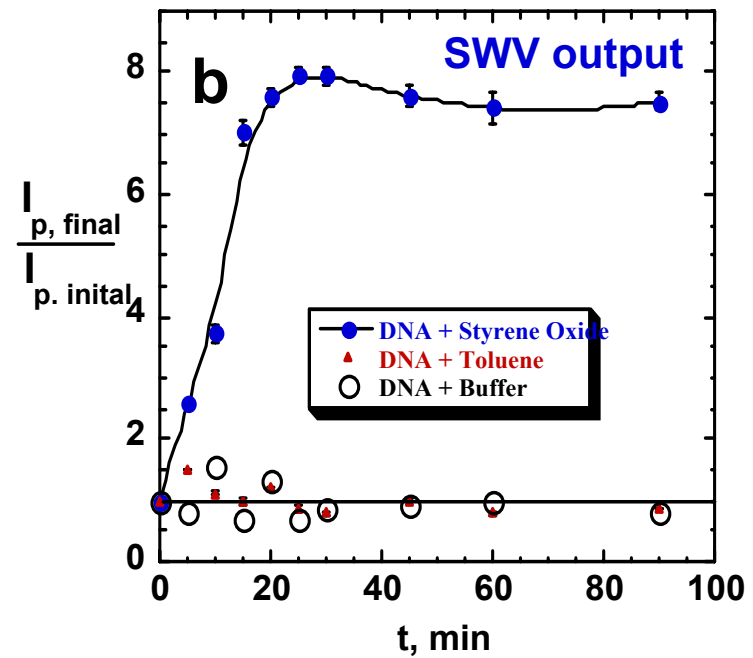
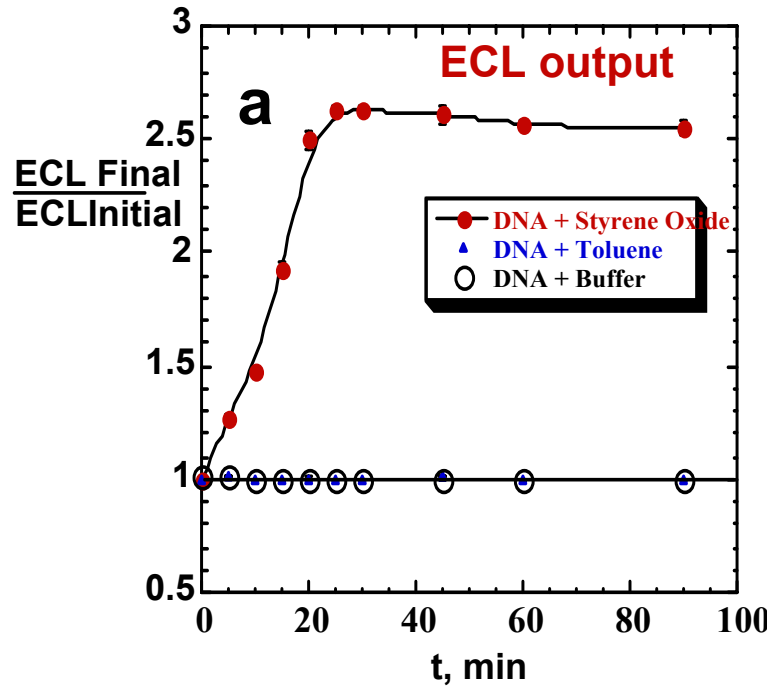
Equipment for ECL toxicity sensors



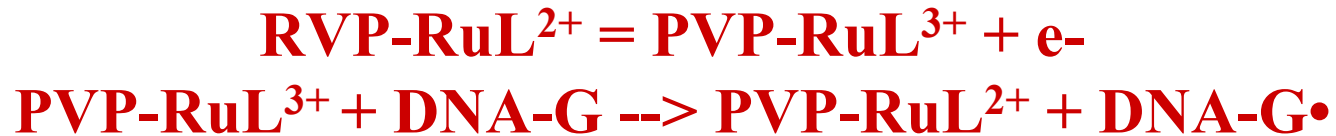
Incubations with styrene oxide



Incubation of Ru-PVP/DNA films with styrene oxide films with styrene oxide



Direct ECL generation from DNA



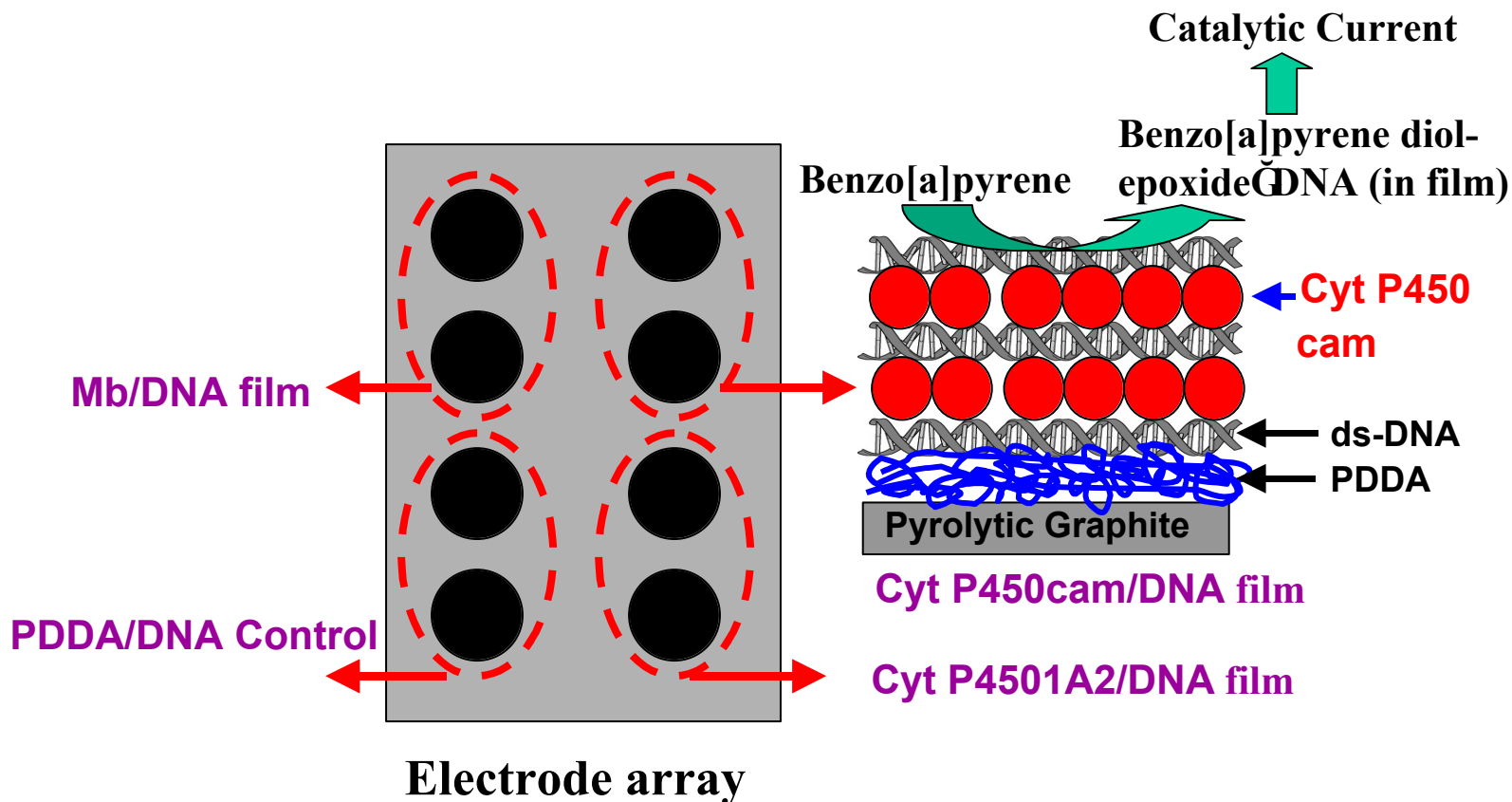
Then?

PVP-RuL³⁺ oxidizes DNA-G[•] to give
Photoexcited PVP-[RuL²⁺]*

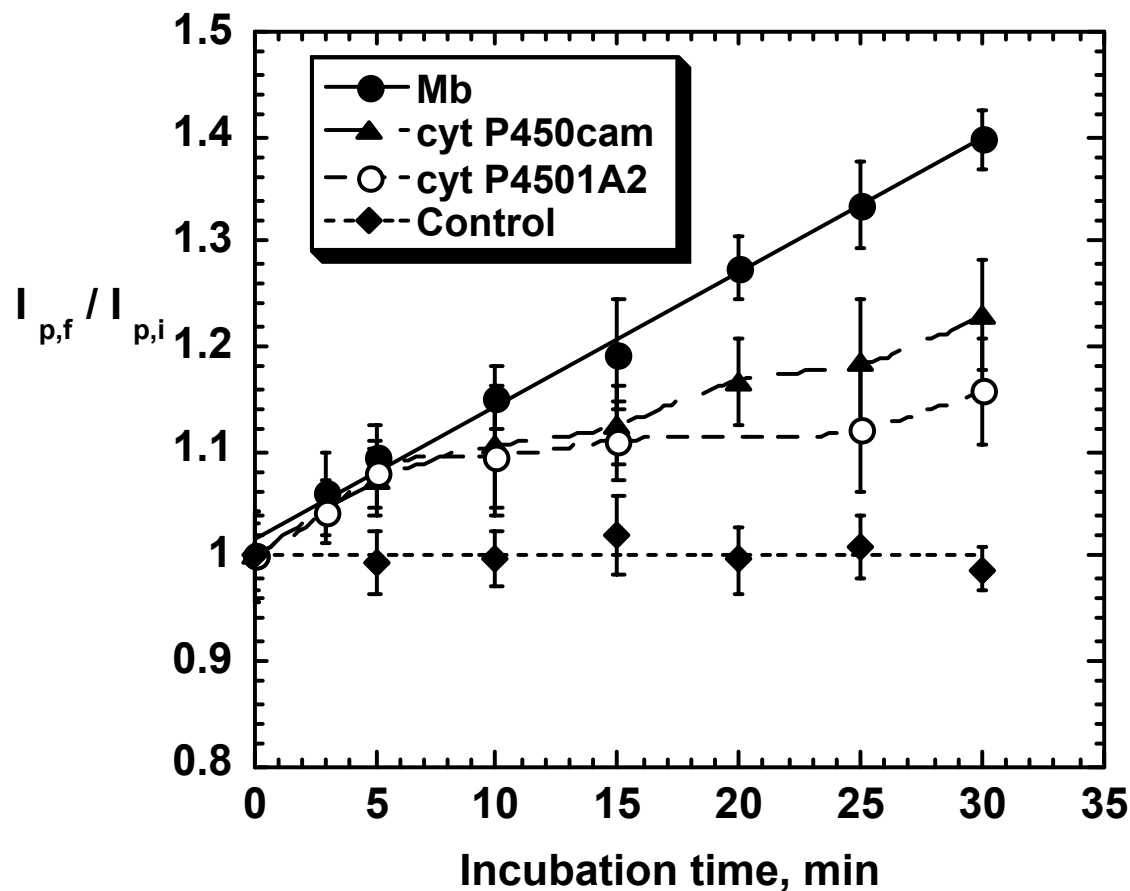
Or

DNA-G[•] reduces PVP-RuL²⁺ to PVP-RuL⁺,
PVP-RuL³⁺ + PVP-RuL⁺ → PVP-[RuL²⁺]*

Arrays: Which Liver Cytochrome P450s - generate toxic Benzo[a]pyrene Metabolites?



Arrays detect in-vitro DNA damage from metabolites of different enzymes in DNA/enzyme films



**Rel. turnover rate,
1/min (nmol E)**

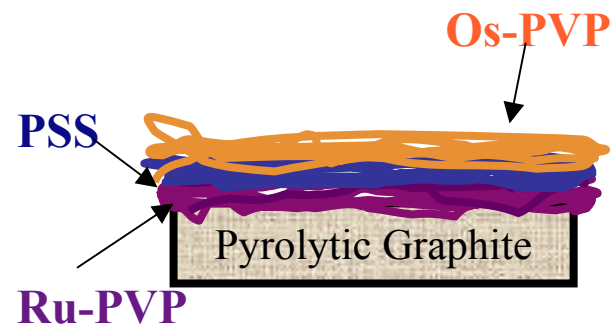
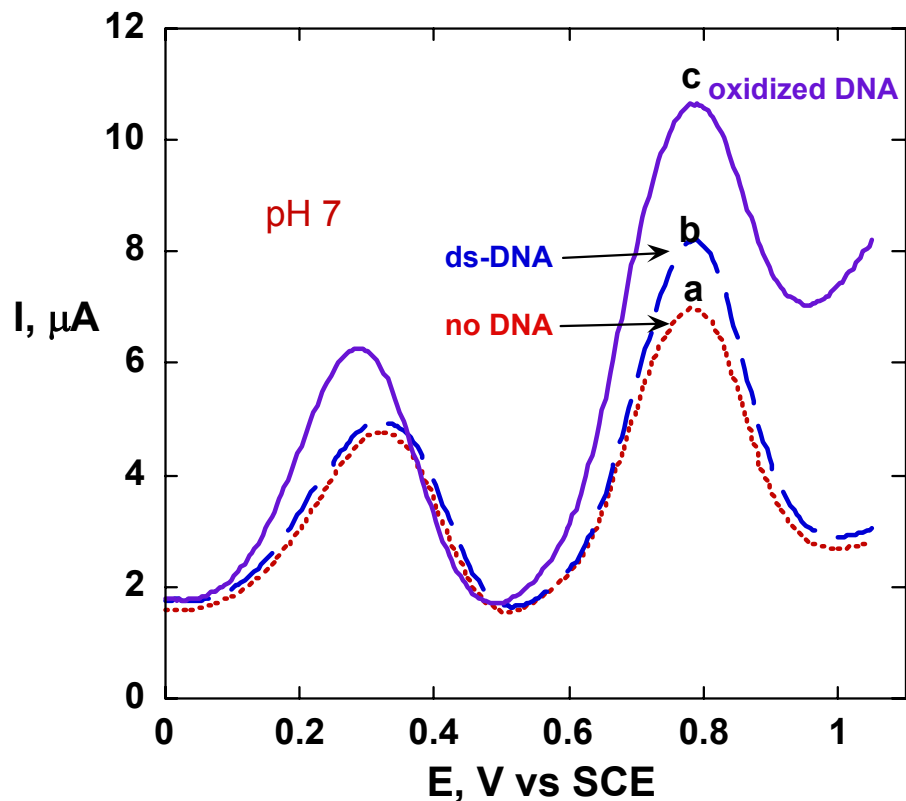
Mb	0.9
P450cam	3.0
P450 1A2	3.5

*Drug discovery
applications*

Figure 7. Influence of incubation time with 50 μM benzo[a]pyrene and 1 mM H_2O_2 on the peak current ratios from SWV of PDDA/DNA/(enzyme/DNA)₂ films Control is PDDA/DNA/(Mb/DNA)₂ film in 50 μM benzo[a]pyrene alone.

Sensors for oxidative stress via oxidized DNA

SWV (10 Hz) of PVP-Ru/PSS/PVP-Os film (a) in buffer;
 (b) + 0.2 mg/mL CT ds-DNA
 (c) + 0.2 mg/mL CT ds-DNA after 80 min. in Fenton reagent



ECL detection in films:

Lynn Dennany, Robert J. Forster, Blanaid White, Malcolm Smyth and James F. Rusling, *Am. Chem. Soc.*, 2004, 126, 8835-8841.

Amos Mugeru, Bingquan Wang and James F. Rusling 'Voltammetric Detection of Oxidized DNA Using Ultrathin Films of Os and Ru Metallopolymers', *Anal Chem* 2004, 76, 5555-5563.

Summary: DNA damage detection/toxicity sensors

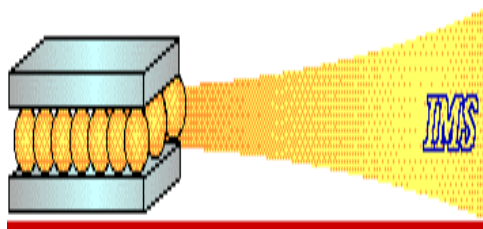
- **Catalytic voltammetry and ECL toxicity sensors**
- **sensors produce metabolites, damage DNA**
- **Can detect 5-10 damaged bases/10,000**
- **can detect DNA oxidation - 8-oxoguanine (1/6000)**
- **Future: extensions to many compounds, cyt P450 arrays, ECL arrays, drug toxicity**

Single-walled carbon nanotube forests as a basis for immunosensors

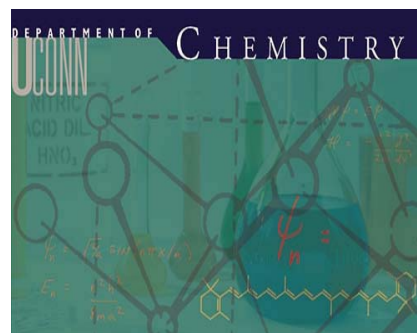
James F. Rusling and Xin Yu,
Depts. of Chemistry and Pharmacology, Univ. Connecticut

Maire O'Connor, Anthony Killard, Malcolm Smyth
NCSR, Dublin City University

Sang Nyon Kim, Fotis Papadimitrakopoulos
Institute of Materials Science, University of Connecticut

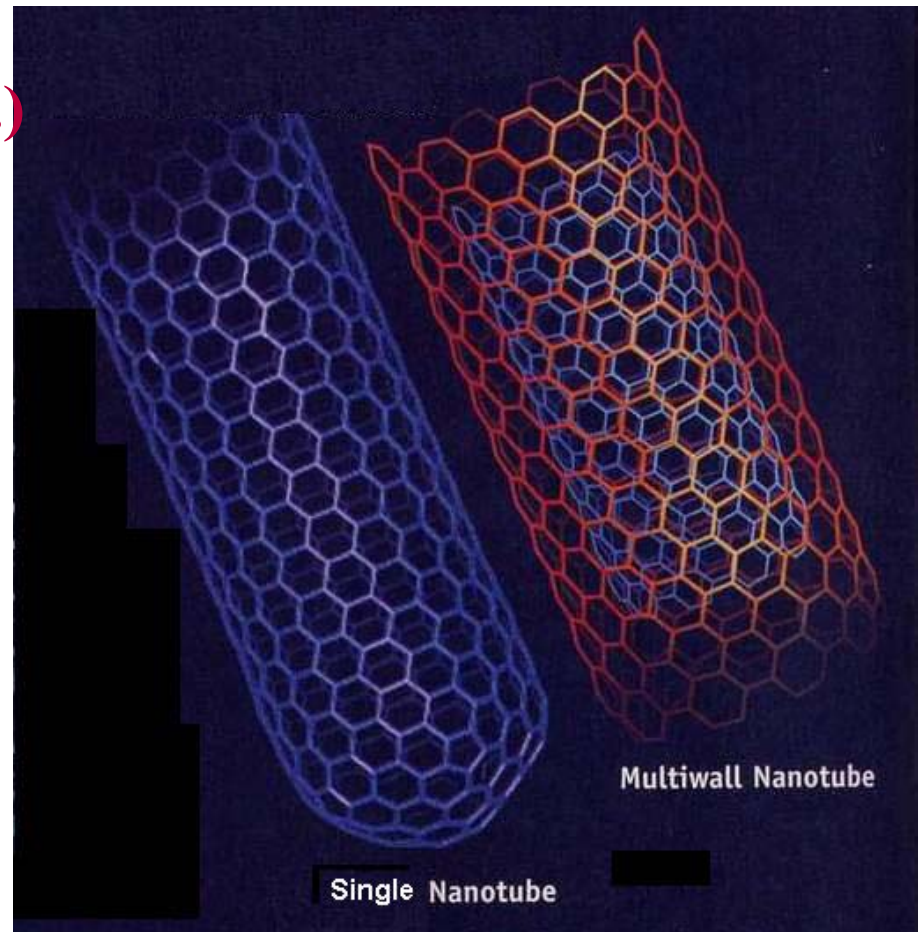


Nanomaterials Optoelectronics Laboratory



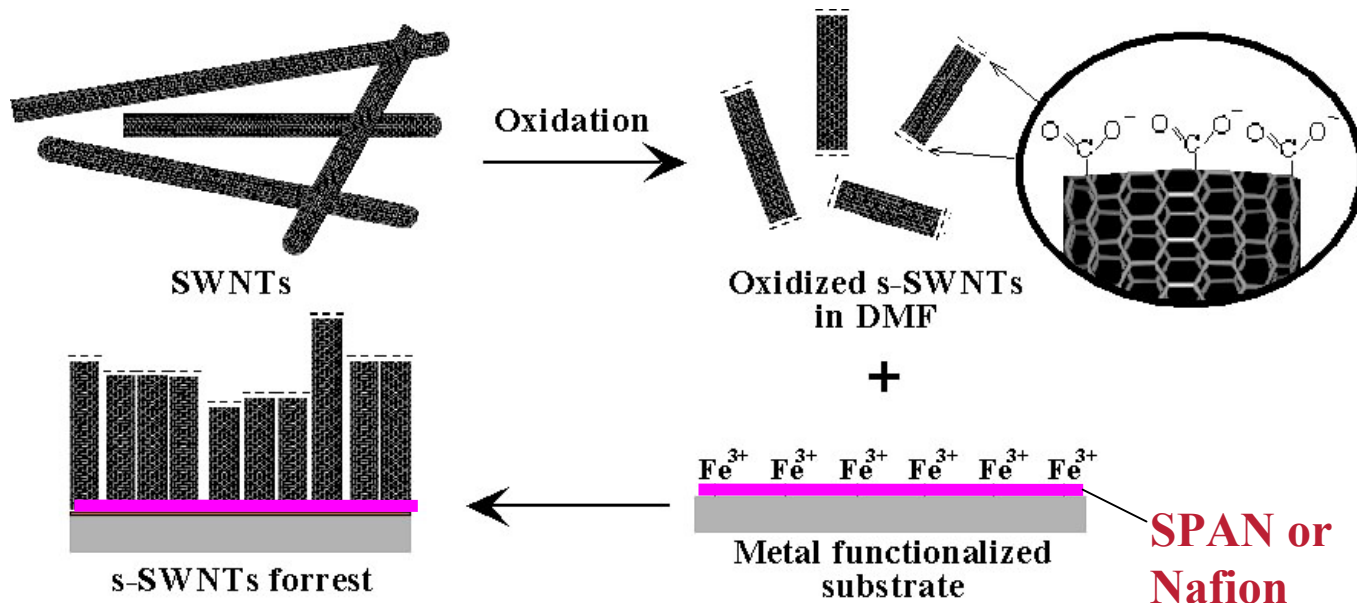
Carbon Nanotubes

- **Single walled (1.4 nm o.d.) and multi-walled**
- **Highly conductive, flexible, strong, patternable**
- **Commercially Available**



Single-Walled Carbon Nanotube Forests: Antigen-Antibody Sensing

~1.4 nm diameter, high conductivity

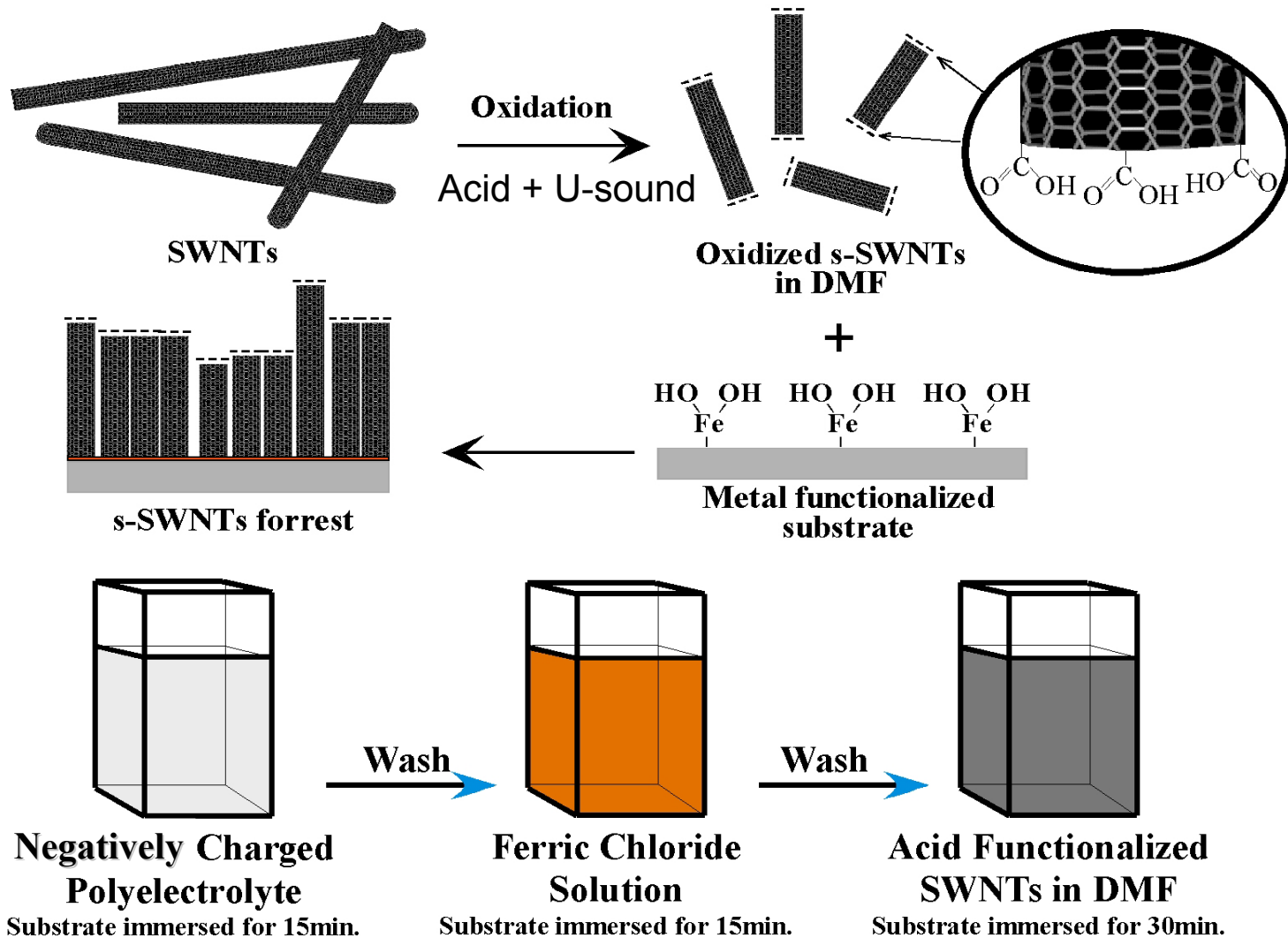


Chattopadhyay, Galeska, Papadimitrakopoulos, *J. Am. Chem. Soc.* 2001, 123, 9451.

End COOH groups allow chemical attachment to proteins (antibodies)

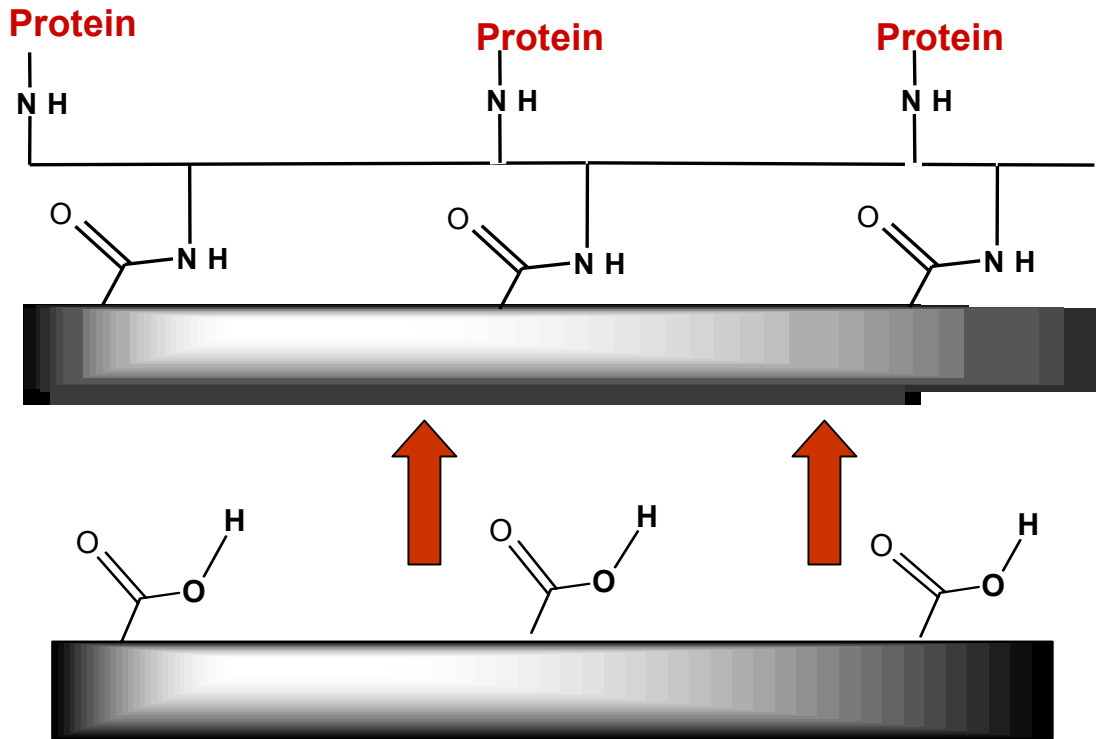
High conductivity to conduct signal (e's) from enzyme label to meas. circuit

Experimental Procedure for SWNT Forest Assembly



Chattopadhyay, Galeska, Papadimitrakopoulos, *J. Am. Chem. Soc.* 2001, 123, 9451.

Covalently Binding Protein to SWNT

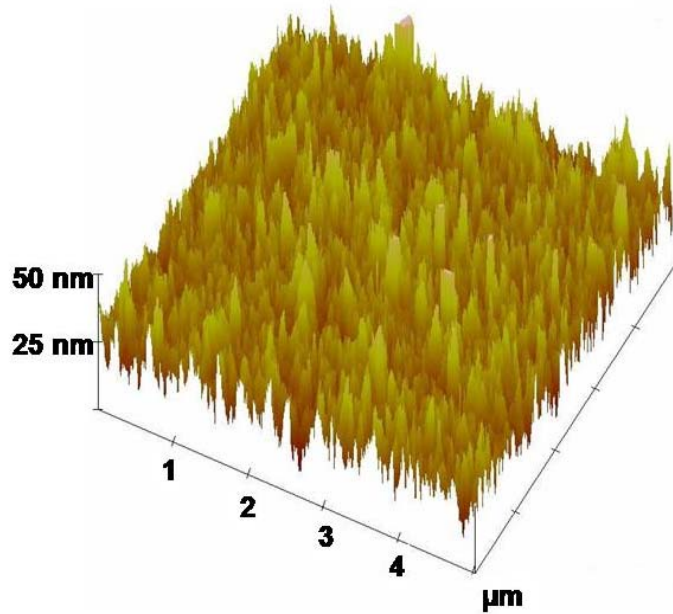


Ends of nanotubes -COOH:

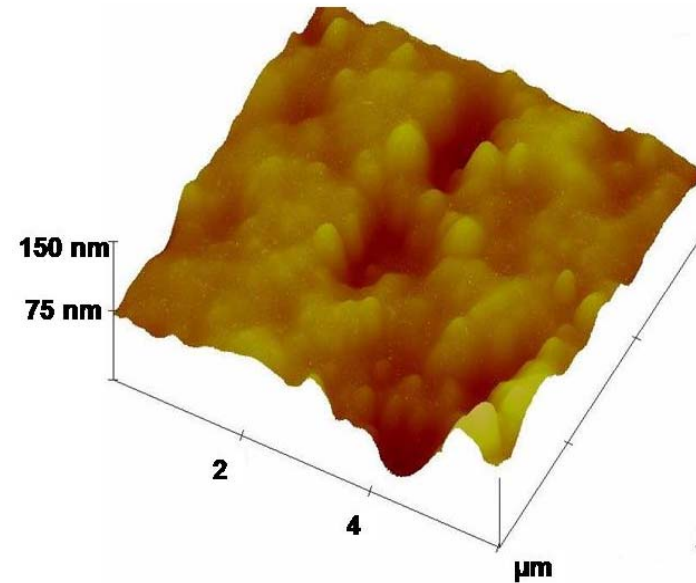
SWNT

water-soluble carbodiimide (1-(3-(dimethylamino) propyl)-3-ethylcarbodiimide hydrochloride, EDC, or EDC + NHSS

AFM of SWNT forest with and without antibody attached



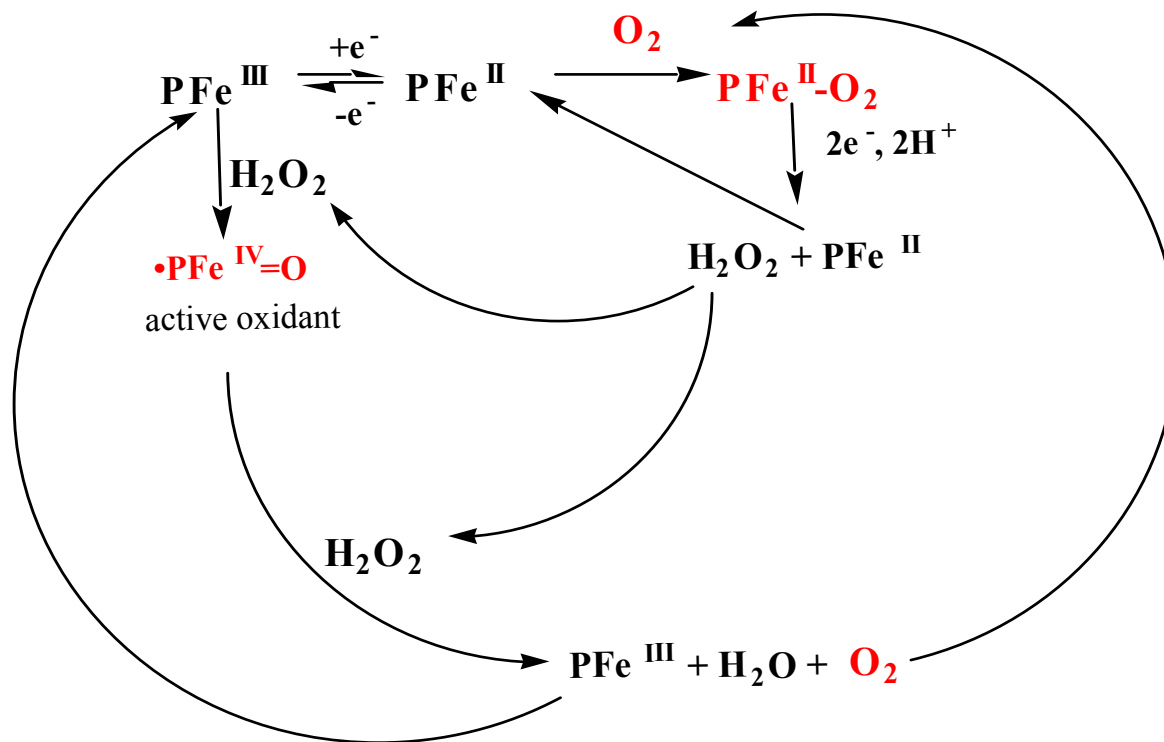
(a) SWNT



(b) SWNT + antibody
(EDC coupling)

(a) SWNT forest on smooth silicon and (b) Anti-biotin antibody functionalized SWNT on smooth silicon

Electrochemical Response of Peroxidases



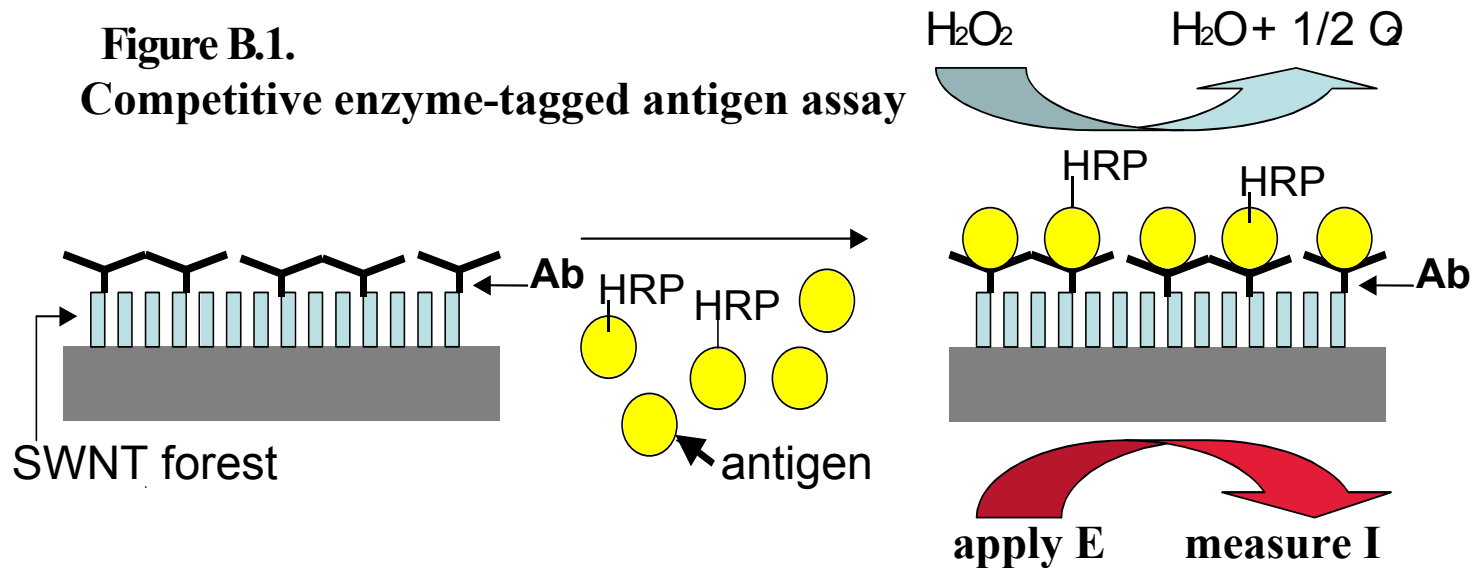
Possible reduced species in red

HRP on electrodes: + H₂O₂ = current signal

Zhe Zhang, Salem Chouchane, Richard S. Magliozzo, and James F. Rusling, "Direct Voltammetry and Enzyme Catalysis with *M. tuberculosis* Catalase-Peroxidase, Peroxidases and Catalase in Lipid Films", *Anal. Chem.*, **2002**, 74, 163-170.

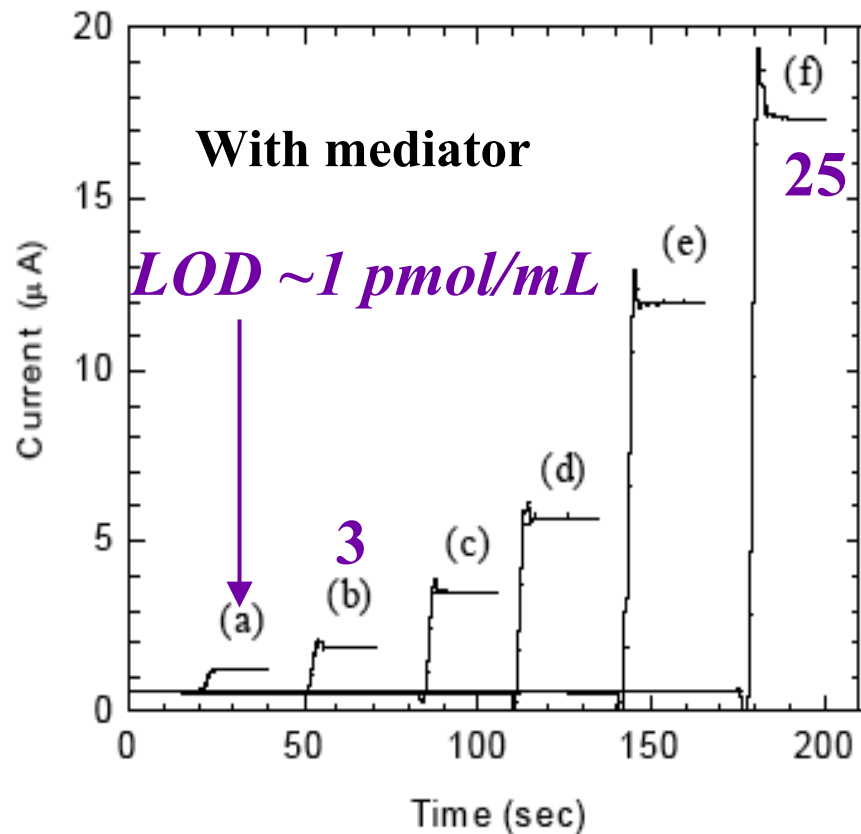
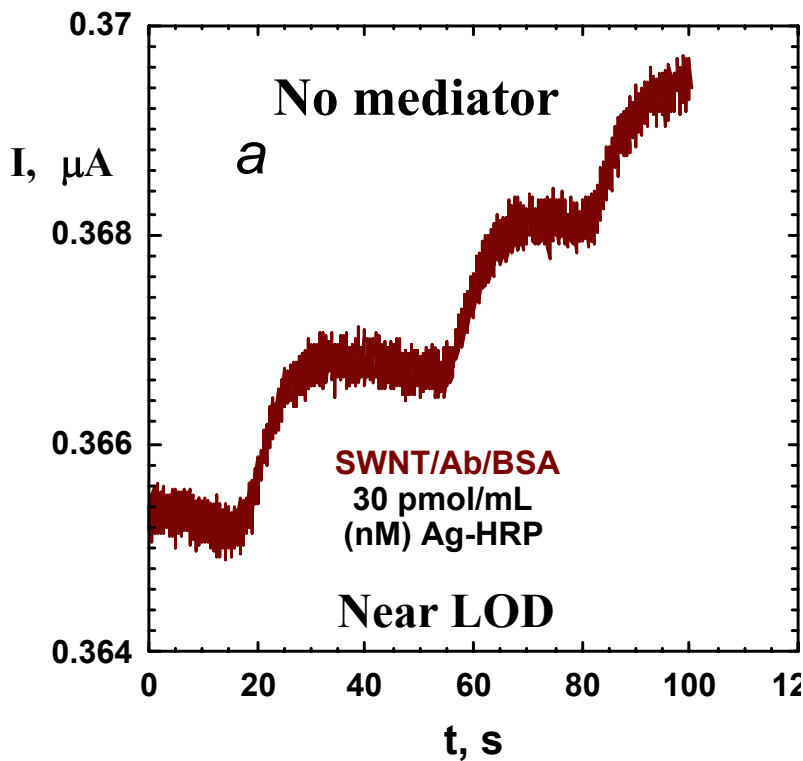
Competitive Immunoassay

Figure B.1.
Competitive enzyme-tagged antigen assay



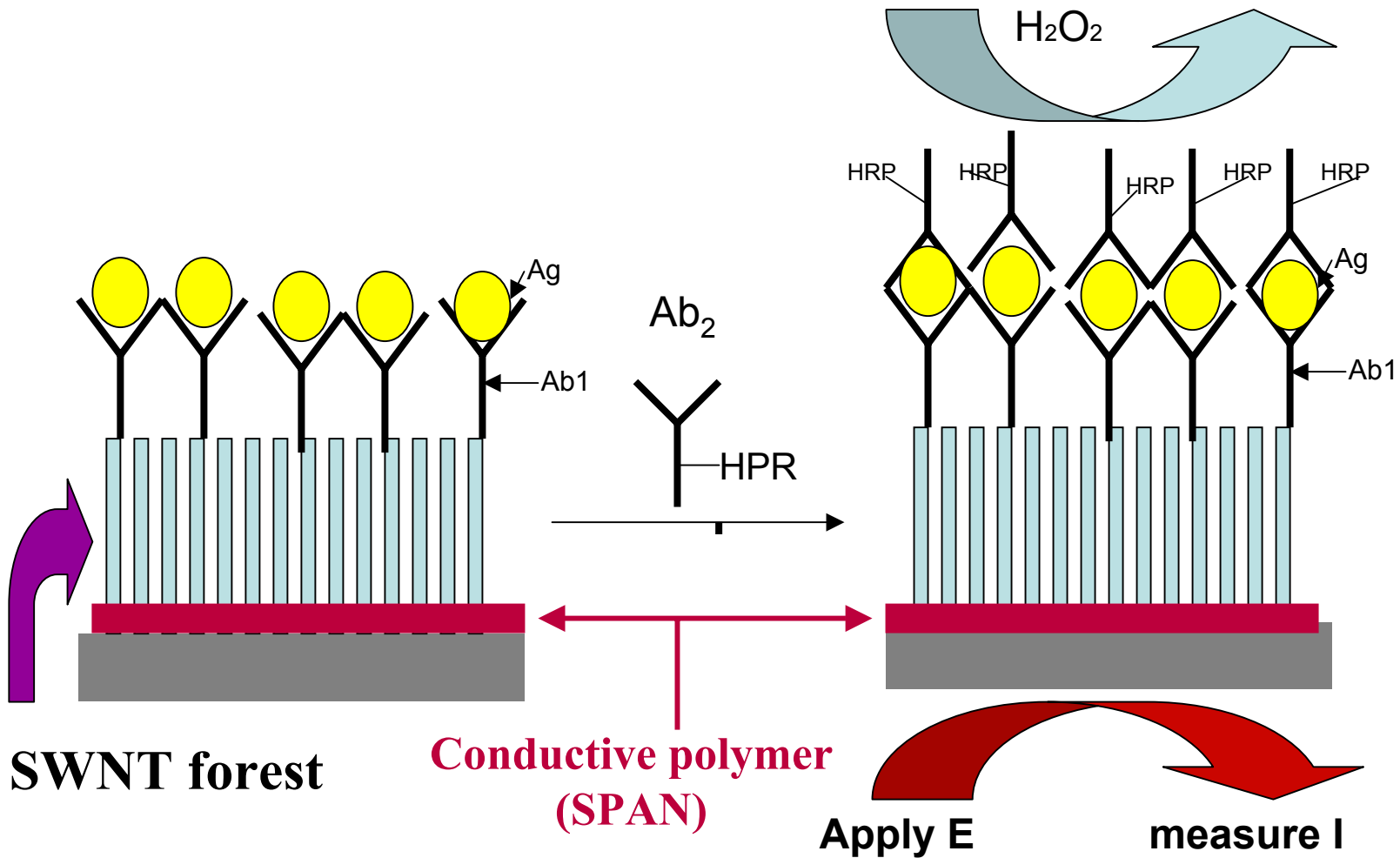
Catalytic current should be inversely proportional to the amount of non-labeled Ag, depending on binding constant, Ag was pre-bound on Ab

Anti-biotin/biotin-HRP test system (H₂O, present)

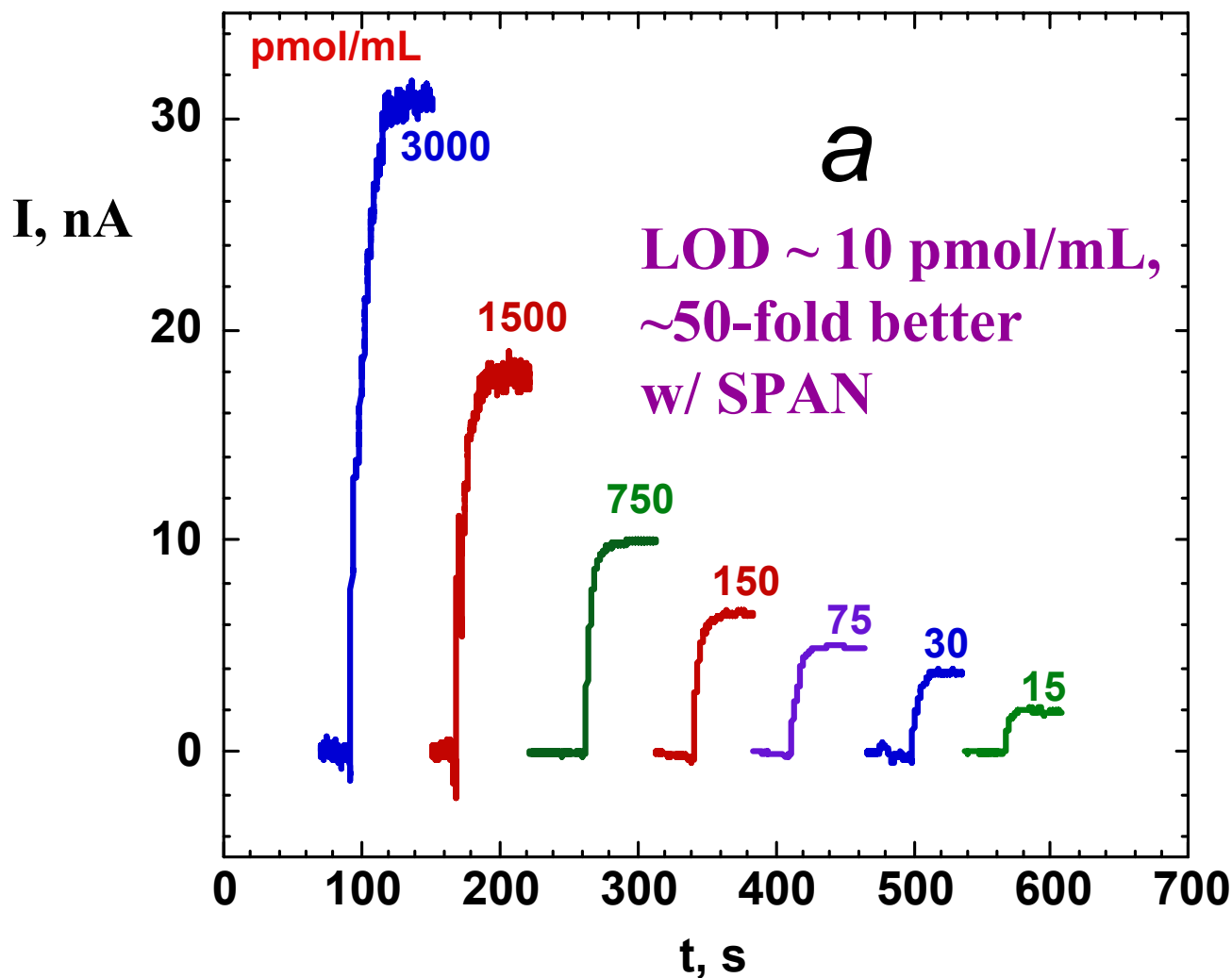


not all the HRP label was communicating
with the measuring circuit - soluble mediator shuttles
electrons from HRP label more efficiently

Sandwich Assay for Human Serum Albumin

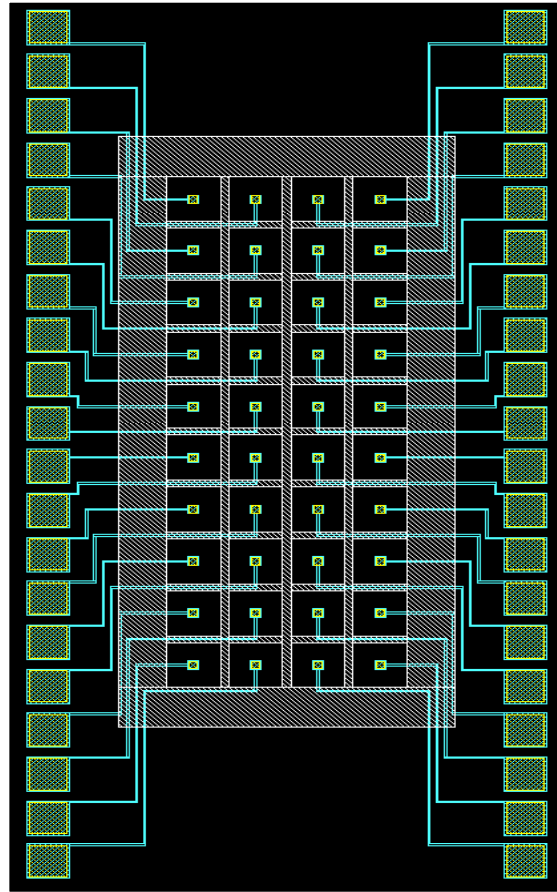


*Detection of Human Serum albumin in
10 μL drops on SWNT forest immunosensor*

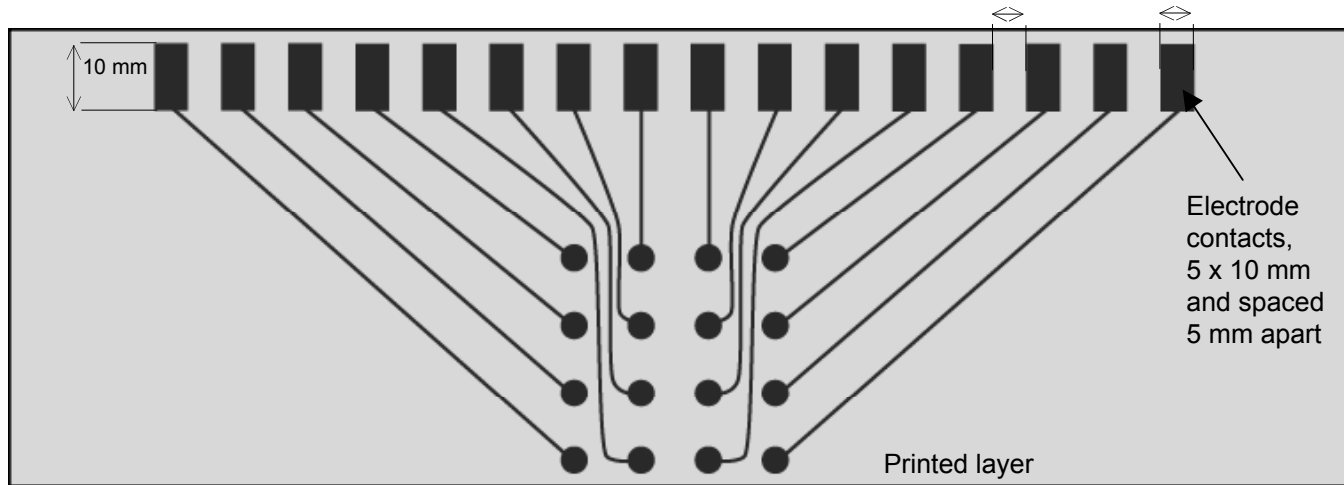


Design approaches to future arrays

1. Layer-by-layer approach general, simple
2. Stable films, complex architecture, any surface
3. Sensors for toxicity, oxidative stress
4. **Ambient T solution processable**
5. SWNT forests patterned by solution process
6. Excellent LOD and sensitivity using conductive polymer bed (SPAN)
7. Possibility of automated array formation
8. Applications to proteins, pathogens, etc.



**Future work: pattern SWNT forest arrays onto microchip
collaboration with Univ. of Edinburgh Genomics Inst. (GT)**



Also, screen printed carbon arrays, Lab 901, Edinburgh

Detection of Protein biomarkers for Cancer:

- **NIH, NIDCR**
- **prostate, squamous cell, and breast cancers**

QuickTime™ and a
TIFF (Uncompressed) decompressor
are needed to see this picture.

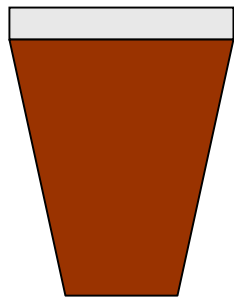
Thanks to NIH, NSF and ARO for funding!

Thanks to all our coworkers and collaborators

<http://web.uconn.edu/rusling/>

Thanks to YOU for listening!

Thanks to intangible creative factors



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